



⑫

EUROPEAN PATENT APPLICATION

⑬ Application number: 87850161.8

⑮ Int.Cl.³: A 61 F 2/16

⑭ Date of filing: 14.05.87

⑩ Priority: 14.05.86 US 862989

⑪ Date of publication of application:
19.11.87 Bulletin 87/47

⑫ Designated Contracting States:
AT BE CH DE ES FR GB GR IT LI LU NL SE

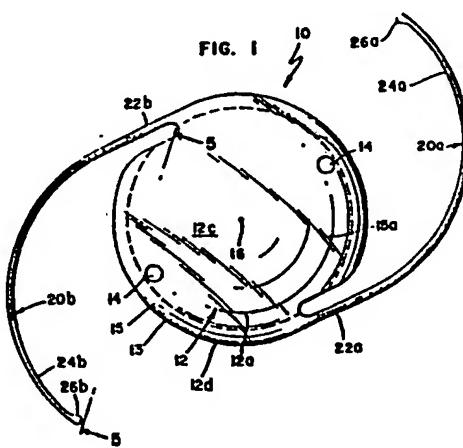
⑬ Applicant: PRECISION-COSMET CO., INC.
11140 Bren Road West
Minnetonka Minnesota 55343(US)

⑭ Inventor: Bissonette, Noel G.
7000 Irving Avenue South
Minneapolis Minnesota 55423(US)

⑮ Representative: Ström, Tore et al.
Ström & Gulliksson AB Studentgatan 1 P.O. Box 4188
S-203 13 Malmö(SE)

⑯ Intraocular lens with tapered haptics.

⑰ An intraocular lens for use as an artificial lens implant is disclosed. The intraocular lens includes an optical lens body (12) having a periphery (13) and two curved, elongated and resilient haptic members (20a, 20b) for positioning and supporting the lens in the eye. Each haptic member has an inner or root end (22a, 22b) and an outer or free end (26a, 26b). The haptic members are integrally formed with the lens body as a one-piece construction at the root ends thereof. The haptic members extend outwardly from the lens body along an arc exterior to the periphery of the lens body. Each haptic member has at least a portion thereof tapered or reduced in cross sectional dimension in a direction therealong from the root end toward the free end.



INTRAOCCULAR LENS WITH TAPERED HAPTICS

TECHNICAL FIELD

This invention relates generally to intraocular lenses to be used as artificial lens implants in eyes from which the cataractous natural lens has been removed, and more particularly to an improved structure 5 for the haptic elements of an intraocular lens.

BACKGROUND

The implantation of an intraocular lens for 10 restoring vision after cataract surgery is well-known in the art. In general, two forms of surgery are used to remove cataracts. These are extracapsular cataract extraction and intracapsular extraction. (Discussed in U.S. Pat. Re. 31,626 to Hoffer) Following extraction of 15 a cataractous lens, an intraocular lens is normally implanted in either the anterior or the posterior chamber of the eye. In an anterior chamber implant, the lens is generally situated forward of, or mounted to the iris. In the case of posterior chamber implants, the 20 lens is situated behind the iris and may be mounted within the cleft or fornix of the capsule which remains in place after extracapsular surgery.

In both anterior or posterior chamber implants, the lens is usually centered and fixed in position by one or more supporting strands or haptic members. While available intraocular lenses incorporate 25 haptic member(s) having various geometric shapes and configurations, the typical haptic member is a flexible strand of non-biodegradable material which is fixed to the lens body, and exhibits specific spring-like memory 30 qualities so that the haptic member can be compressed or off set from the normal rest position and thereafter returned to the fully extended condition when pressure is removed. (See U.S. Patent No. 4,468,820 to Uhler et 35 al.; U.S. Patent No. 4,435,855 to Pannu; and U.S. Patent No. 4,494,254 to Lopez.)

The typical diameter or thickness of a haptic member is about 0.1-0.2 mm; and therefore requires careful handling prior to and during implantation of the lens. For example, a haptic member can break or weaken 5 when improperly handled with a surgical instrument, such as forceps. A broken haptic renders the lens useless. In the case of an integral one-piece lens a broken haptic requires that an entirely new lens be used.

While not common, it is possible that improper 10 handling of a haptic prior to lens implantation may damage the haptic without breaking it. If a lens with a damaged haptic is implanted and the haptic breaks subsequent to surgery, serious complications can arise. Dislocation of a lens subsequent to surgery could 15 seriously impair vision and/or damage the eye.

Among the wide variety of intraocular lenses having haptic support members, all known haptics have a uniform cross sectional dimension or thickness. When 20 pressure is applied to the haptic (i.e. grasping root or base area of haptic with forceps) stress is concentrated at a relatively small area, thereby increasing the potential for breakage in the area of concentrated stress.

It is well known that distortion of the 25 eyeball can be caused by normal physical activities such as walking or rubbing the eyelids, as well as by more severe physical contact such as falls or collisions. When an intraocular lens has been implanted, distortion of the eyeball can place intermittent stress on the haptic members. This intermittent stress generally results 30 in eye irritation, redness or other minor trauma. It is believed that these intermittent stresses can be minimized by increasing the flexibility of the haptic members. However, if haptics of the type currently 35 available are made thinner to increase flexibility, the

potential for breakage is also increased.

Accordingly, a substantial need exists for a haptic support member which exhibits high resistance to breakage when handled. The present invention provides 5 an artificial lens having an improved haptic member which is strengthened to minimize breakage. The strengthened haptic member of the present invention also provides for thinner more flexible haptics without sacrificing needed strength.

10

SUMMARY OF INVENTION

The present invention is an intraocular lens for use as an artificial lens implant in an eye. The 15 intraocular lens has an optical lens body and an improved means for positioning and supporting the lens body in the eye. Particularly, the lens body of the present invention is positioned and supported in the eye by at least one resilient haptic member having a root 20 end and a free end. The haptic member is connected to the periphery of the lens body at the root end thereof. Preferably, the haptic member and lens body are integrally formed as a one-piece construction at the root end. The haptic member extends outwardly from the 25 lens body along an arc exterior to the periphery of the lens body and is strengthened by having at least a portion thereof tapered in a direction along its length from the root end toward the tip. The tapered portion of the haptic member distributes externally applied 30 stresses over a substantial length of the haptic member, thereby avoiding concentration of stress and minimizing the potential for breakage in the area of concentrated stress.

In a preferred embodiment of the present 35 invention, two curved elongated and resilient haptic members are integrally formed with the lens body at the

periphery thereof. The two haptic members extend tangentially therefrom along an arc exterior to the periphery and have a cross sectional dimension which is reduced over at least a portion thereof in a direction 5 along the length of the haptic from the root end toward the free end.

In one embodiment of the present invention, the haptic members have a circular cross section which is reduced along all dimensions of the haptic in a 10 direction along the entire length from the root end to the tip of the free end. In an alternate embodiment, the haptic members have a circular cross section which is reduced only over a portion of each haptic in the direction therealong from the root end toward the free 15 end.

In all preferred embodiments, the haptic members or members are tapered proximate the root end in the direction from the root end toward the free end. Inclusion of a tapered portion in at least the area of 20 the root end increases the haptic's resistance to fracturing without compromising flexibility.

The present invention makes possible thinner, more flexible haptics which can withstand greater deformation without fracturing. More flexible haptics such 25 as provided for by the tapered haptics of the present invention can: adapt to distortion of the eye resulting from activities such as rubbing and pressing; deflect independently; adapt to the shape of the eye to equalize pressure; uniformly deflect in a plane perpendicular to 30 the plane of the optic of the lens; control deflection forces over a broad area of the eye; and reduce tenderness in the eye. Accordingly, the advantages of increased flexibility made possible by the present invention provide for a safer, more comfortable and 35 better performing intraocular lens.

These and various other advantages and features of the novelty which characterizes the invention are pointed out with particularity in the claims annexed hereto and forming a part hereof. However, for better understanding the invention, its advantages, and objects attained by its use, reference should be had to the drawings which form a further part hereof and to the accompanying descriptive matter in which there is illustrated and described a preferred embodiment of the invention.

BRIEF DESCRIPTION OF THE DRAWING

FIG. 1 is a top plan view of a preferred embodiment of the intraocular lens of the present invention;

FIG. 2 is a side elevational view of the lens shown in FIG. 1.

FIG. 3 is a top plan view of a prior art intraocular lens.

FIG. 4 is a side elevational view of the prior art lens shown in FIG. 3.

FIG. 5 is an elevational view taken along the line 5-5 in FIG. 1 showing one embodiment of the taper of the haptic member of the present invention.

FIG. 6 is a sectional view taken along line 6-6 in FIG. 5.

FIG. 7 is a sectional view taken along line 7-7 in FIG. 5.

FIG. 8 is a top plan view of an alternate embodiment of the intraocular lens of the present invention.

FIG. 9 is a top plan view of still another embodiment of the intraocular lens of the present invention.

FIG. 10 is a simplified cross sectional schematic view of an eyeball with the lens of the present

invention implanted in the posterior chamber.

FIG. 11 is a simplified cross sectional schematic view of an eyeball implanted with the lens of the present invention implanted in the anterior chamber.

5

DETAILED DESCRIPTION OF THE INVENTION

Referring to the drawings, wherein like numerals represent like parts throughout the several 10 views, an intraocular lens designated generally as 10 incorporating the present invention is shown in FIGS. 1, 2 and 5-7.

The intraocular lens 10 includes a central optical region or lens body 12 which preferably, 15 although not necessarily, is of a plano-convex cross-section. As shown in FIGS. 1 and 2, the optical lens body 12 has an upper portion 12c with an anteriorly convex upper surface 12a and a base portion 12d with a posteriorly substantially planer bottom surface 12b. 20 The base portion 12d is relatively thin compared to the upper portion 12c. The optical lens body 12 has an apex 16, and a peripheral zone 15 including the outer periphery or circumference 13 of the lens body 12. The peripheral zone 15 is exterior to the optical zone 15a 25 of the lens. The lens body 12 has a height h' as shown in FIG. 2, of a distance between the apex 16 and the bottom surface 12b. The height h' can be characterized as the distance from the apex 16 to the bottom surface 12b measured along the optical axis 24 of lens body 12. 30 Interconnected to the periphery 13 of the lens body 12 are two curved elongated haptic members 20a,b extending outwardly from the lens body 12 along an arc exterior to the periphery 13. While the haptic members 20a,b as shown in FIG. 1, extend from the periphery 13 it is to be 35 understood that the haptic members could extend out-

wardly from points anywhere within the peripheral zone

15.

The lens body 12 of the lens 10 is centered and retained within the eye by the flexible haptic members 20a,b. As shown in FIG. 1, the haptic members 20a,b include root ends 22a,b connected to the periphery 13 of the lens body 12 and outer or free ends 24a,b which each terminate at a tip 26a,b. In the preferred embodiment shown in FIG. 1 the cross sectional dimension or diameter of the tip 26a,b is slightly enlarged to minimize irritation to the eye. Particularly, the curved haptics with rounded ends fit snugly but comfortably inside the eye but avoid single point pressure which can lead to undesired complications, such as zonule rupture or ciliary body pressure in posterior chamber implants.

In the preferred embodiment shown in FIG. 1, the haptic members 20a,b are spaced and located approximately across the diameter of the lens body 12. While the haptic members 20a,b may be connected to the lens body 12 at the periphery 13 thereof by a number of known methods, in the preferred embodiment shown, the haptic members 20a,b and the lens body 12 are formed as an integral one-piece structure by forging and machining process. However, it will be appreciated that the lens 10 may also be produced by other suitable methods such as injection molding and lathing.

In the preferred embodiment of FIGS. 1 and 2 the arc traversed by the haptic members 20a,b is substantially circular and curved toward the periphery 13 of the lens body 12. It is to be appreciated that arcuate shaped haptics of a wide variety of shapes and designs are known such as "J" shaped (U.S. Patent No. 4,468,820 to Uhler et al; U.S. Patent No. 4,435,855 to 35 Pannu) and "C" shaped (U.S. Patent No. 4,477,931 to Kelman; U.S. Patent No. 4,494,254 to Lopez). The lens

of the present invention could incorporate haptics with any of these known shapes and designs, including a single haptic member or a combination of a single flexible haptic member together with an inflexible haptic support element.

5 The haptic members 20a,b are easily compressed and held in a deformed condition thereby facilitating insertion of the lens into the eye. Particularly, the resilient haptic member members 20a,b 10 spontaneously tend to return to a normal position when released after being forced into the deformed position. This provides an intraocular lens which when positioned in the eye is self-fixating and self-centering and displays less of a tendency to tilt after being 15 implanted in the eye.

The intraocular lens body 12 is made of a biologically tolerable and optically suitable material such as polymethylmethacrylate (PMMA). The haptic members 20a,b are made of a flexible, compressible, resilient plastic material such as PMMA or polypropylene. 20 Preferably, the entire lens 10 is made as an integral one-piece structure of PMMA.

A prior art lens, including haptic members 30a,b with the known uniform cross sectional dimension 25 is shown in FIGS. 3 and 4. In contrast to the known structure for haptic members, according to the present invention the lens 10 is provided with haptic members 20a,b having at least a portion thereof tapered (i.e. reduced in cross sectional dimension) in the direction 30 along the length from the root ends 22a,b toward the free ends 24a,b.

The preferred embodiment shown in FIGS. 1 and 2 includes fiber like haptic members 20a,b tapered along all dimensions of the length from the root ends 35 22a,b to the rounded tips 26a,b of the free ends 24a,b. More particularly, each of the haptic members 20a,b

extends tangentially from the periphery 13 along a substantially circular arc exterior to the periphery 13. Each haptic 20a and 20b traverses an arc of about 140°. Each haptic member 20a and 20b has a circular cross section which is reduced along all dimensions of the haptic fiber, as best shown in FIGS. 5-7. While the preferred embodiment shown in FIGS. 1, 2 and 5-7 includes haptics having a circular cross section, other geometric shapes can be employed by one skilled in the art. By way of example only the cross sectional dimension for the tapered haptic can be rectangular, square or oval.

It is to be understood that while the preferred embodiment in FIGS. 1 and 2 shows haptic members tapered from the root ends 22a,b toward the free ends 24a,b over substantially the entire length of the haptics 20a,b the haptic members need only be tapered over a portion thereof in a direction along the length from the root ends 22a,b toward the free ends 24a,b in order to increase resistance to fracturing. The cross sectional dimension of a partially tapered haptic will be smaller at the free end than at the root end or base.

An alternate embodiment 10' is shown in FIG. 8 in which only a portion of the haptic members 20a',b' is tapered along the length from the root ends 22a',b' in the direction of the tips 26a',b'. In FIG. 8, the taper or area of reducing cross section of the haptic members 20a',b' extends only from root ends 22a',b' to outer points 21a',b' along the length of the haptic members. While extending the area of taper over a greater portion of the haptic increases flexibility, it is to be understood that in order to significantly strengthen the resistance of the haptic member to breakage, only the portion of the haptic substantially adjacent or proximate the root ends 22a,b need be tapered.

In another alternate embodiment not shown, substantially rectangular haptic members having one sur-

face facing the periphery of the lens body and an opposite surface facing away from the periphery may be tapered by reducing the distance between the periphery facing and periphery opposing surfaces over at least a 5 portion of each haptic member along the length from the root end toward the free end.

Providing an intraocular lens with the tapered haptic of the present invention provides for a more even distribution of stress over the length of the haptic 10 member than is exhibited by a haptic member having a uniform cross sectional dimension along its entire length as seen in FIGS. 3 and 4. An intraocular lens with a tapered haptic member also makes possible thinner more flexible haptics without compromising strength. 15 By way of example, a typical haptic such as seen in FIGS. 3 and 4 has a diameter between 0.01 and 0.02 mm. over the entire length of the fiber. In contrast to this, haptics 20a,b such as seen in FIG. 1 can be tapered from 0.15 to 0.08 mm in the direction from the 20 root ends 22a,b toward the free ends 24a,b. The thinner tapered haptic not only exhibits greater flexibility but also possesses greater resistance to fracture. More flexible haptics in accordance with the present invention will ease handling of the lens prior to and during 25 positioning in the eye and provide for more comfortable and better performing lens.

The present invention is applicable to intraocular lenses 10 of all geometric shapes and configurations. Intraocular lenses 10 including the 30 tapered haptics 20a,b of the present invention can be adopted for use as both posterior chamber intraocular lens implants as seen in FIG. 10 as well as anterior chamber intraocular lens implants as seen in FIG. 11.

The preferred embodiment of the lens 10 shown 35 in FIG. 1 is of the type designed for posterior chamber implantation and includes an annular lip 17 projecting

only rearwardly from the bottom surface 12b. When the lens 10 is implanted in the posterior chamber 42 as seen in FIG. 10 the annular lip 17 sits against the posterior capsule 46 and creates a space between the capsule 46 and rear of the optical zone 15a of the lens body 12. 5 The preferred embodiment shown in FIG. 1 also includes positioning holes 14.

The posterior chamber type lens 10 will typically be utilized following extracapsular cataract extraction. 10 As illustrated in FIG. 10, the lens 10 is implanted in a human eye 40, in the posterior chamber 42 behind the iris 44. Preferably, the cataract has been extracted from the capsular bag 46, leaving intact the posterior wall 46a and an annular flap portion 46b 15 forming a cleft or fornix 46c. The capsular bag 46 is connected to the ciliary muscle in the eye wall 48 via suspensory ligaments 50. Vitreous humor in the region 52 behind the capsular bag 46 is prevented from flowing forward by the posterior wall 46a which assumes a 20 generally planar shape.

When the lens 10 is implanted in the posterior chamber of the eye, as seen in FIG. 10 the haptic elements 20a,b support the lens 10 by engaging the cleft or fornix portion 46c; thereby fixating the position 25 of the lens 10 in the eye 40.

When the lens 10 is adapted to be implanted in the anterior chamber of the eye 40 as seen in FIG. 11, the haptic members 20a",b" support the lens 10" in a spaced relationship anterior to the iris 44 of the eye 30 40. Specific design characteristics of a lens suitable for implanting in the anterior chamber, such as proper curvature of the haptic members 20a",b" and the determination of the angle at which the haptics 20a",b" project from the lens body 12" are known by those skilled in the 35 art. One embodiment of an anterior chamber lens is shown in FIG. 9, and parts thereof similar to lens 10 carry similar numbers with double prime ("') marks added.

While the above embodiments have been described with reference to a plano-convex lens, it is understood that the improved haptic member is also applicable to bi-convex lenses. The bi-convex lens 5 would have a convex upper surface and convex bottom surface. The tapered haptics of the present invention could also be utilized with plano-concave lenses. Other modifications of the invention will be apparent to those skilled in the art in light of the foregoing description. 10 This description is intended to provide specific examples of individual embodiments which clearly disclose the present invention. Accordingly, the invention is not limited to these embodiments or to the use of elements having specific configurations and shapes as 15 presented herein. All alternative modifications and variations of the present invention which follows in the spirit and broad scope of the appended claims are included.

WHAT IS CLAIMED:

1. An intraocular lens comprising;
 - 5 (a) an optical lens body;
 - (b) means for positioning and supporting said lens body in an eye, including at least one resilient haptic member having a root end connected to said lens body and a free end, extending outwardly from said lens body with at least a portion thereof tapered in a direction therealong from said root end toward said free end.
- 10
- 15 2. An intraocular lens according to claim 1 wherein said haptic member is integrally formed with said lens body as a one-piece construction at said root end.
- 20 3. An intraocular lens according to claim 1 wherein said haptic member is fiber like and tapered along all dimensions from said root end to a tip of said free end, said free end having a smaller cross sectional dimension than said root end.
- 25 4. An intraocular lens according to claim 1 wherein said haptic member extends tangentially from a periphery of said lens body.
- 30 5. An intraocular lens according to claim 4 wherein said haptic member has a cross sectional dimension which is reduced over at least a portion thereof in a direction therealong from said root end toward said free end.
- 35 6. An intraocular lens according to claim 5 wherein said haptic member has at least a surface facing

said periphery and an opposite surface facing away from said periphery with the distance therebetween reduced over at least a portion thereof in a direction therealong from said root end toward said tip.

5

7. An intraocular lens according to claim 1 wherein said haptic member has a circular cross section which is reduced along all dimensions over at least a portion thereof in a direction therealong from said root 10 end toward said free end.

8. An intraocular lens according to claim 1 wherein said lens body is made from a biologically tolerable, optically suitable material.

15

9. An intraocular lens according to claim 8 wherein said lens and said haptic member are made of polymethylmethacrylate.

20 10. An intraocular lens suitable for use as an artificial lens implant in an eye; the lens comprising;

(a) an optical lens body having a periphery;
(b) two curved elongated and resiliant haptic members for positioning and supporting said lens in the eye, said haptic members each having a root end and a free end, said haptic members being connected to the periphery of said lens body at said root end thereof and extending outwardly from said lens body along an arc exterior to the periphery of said lens body, said haptic members each having at least a portion thereof tapered in a direction therealong from said root end toward said free end.

35 11. An intraocular lens according to claim 10 wherein said haptic members are integrally formed with

said lens body as a one-piece construction at said root end.

12. An intraocular lens according to claim 10
5 wherein said haptic members are positioned substantially
opposite one another.

13. An intraocular lens according to claim 10
wherein said haptic members are fiber like and tapered
10 along all dimensions from said root end to a tip of said
free end, said free end being smaller in cross sectional
dimension than said root end.

14. An intraocular lens according to claim 10
15 wherein each said haptic member extends tangentially from
said periphery.

15. An intraocular lens according to claim 10
wherein each said haptic member has a cross sectional
20 dimension which is reduced over at least a portion
thereof in a direction therealong from said root end
toward said free end.

16. An intraocular lens according to claim 10
25 wherein each said haptic member has at least a surface
facing said periphery and an opposite surface facing
away from said periphery with the distance therebetween
reduced over at least a portion thereof in a direction
therealong from said root end toward said free end.

30
17. An intraocular lens according to claim 10
wherein each said haptic member has a circular cross
section which is reduced along all dimensions over at
least a portion thereof in a direction therealong from
35 said root end toward said free end.

18. An intraocular lens according to claim 10 wherein said lens body is made from a biologically tolerable, optically suitable material.

5 19. An intraocular lens according to claim 10 wherein said lens and said haptic members are made of polymethylmethacrylate.

10 20. An introcular lens according to claim 10 wherein at least one of said free ends of said haptic members terminates at a tip having an enlarged cross sectional dimension.

15 21. An intraocular lens suitable for use as an artificial lens implant positioned in the posterior chamber of an eye; adjacent the posterior capsule; the lens comprising;

20 (a) an optical lens body having a periphery, upper and bottom surfaces and a generally annular lip projecting only rearwardly from said bottom surface so as to space said lens body from the posterior capsule when said lens is positioned in the posterior chamber;

25 (b) two curved elongated fiber like haptic members for positioning and supporting said intraocular lens in the eye, said haptic members each having a root end and a free end including a tip, said root ends being integrally formed with said lens body
30 to form a one-piece lens, said haptic members extending tangentially from said lens body along an arc exterior to the periphery of said lens body, said haptic members further being resilient so as to spontaneously tend to return to a normal position when released after being forced into a deformed position and having at least a portion

thereof tapered in a direction therealong from said root end toward said free end to strengthen said haptic members.

1/4

FIG. 1

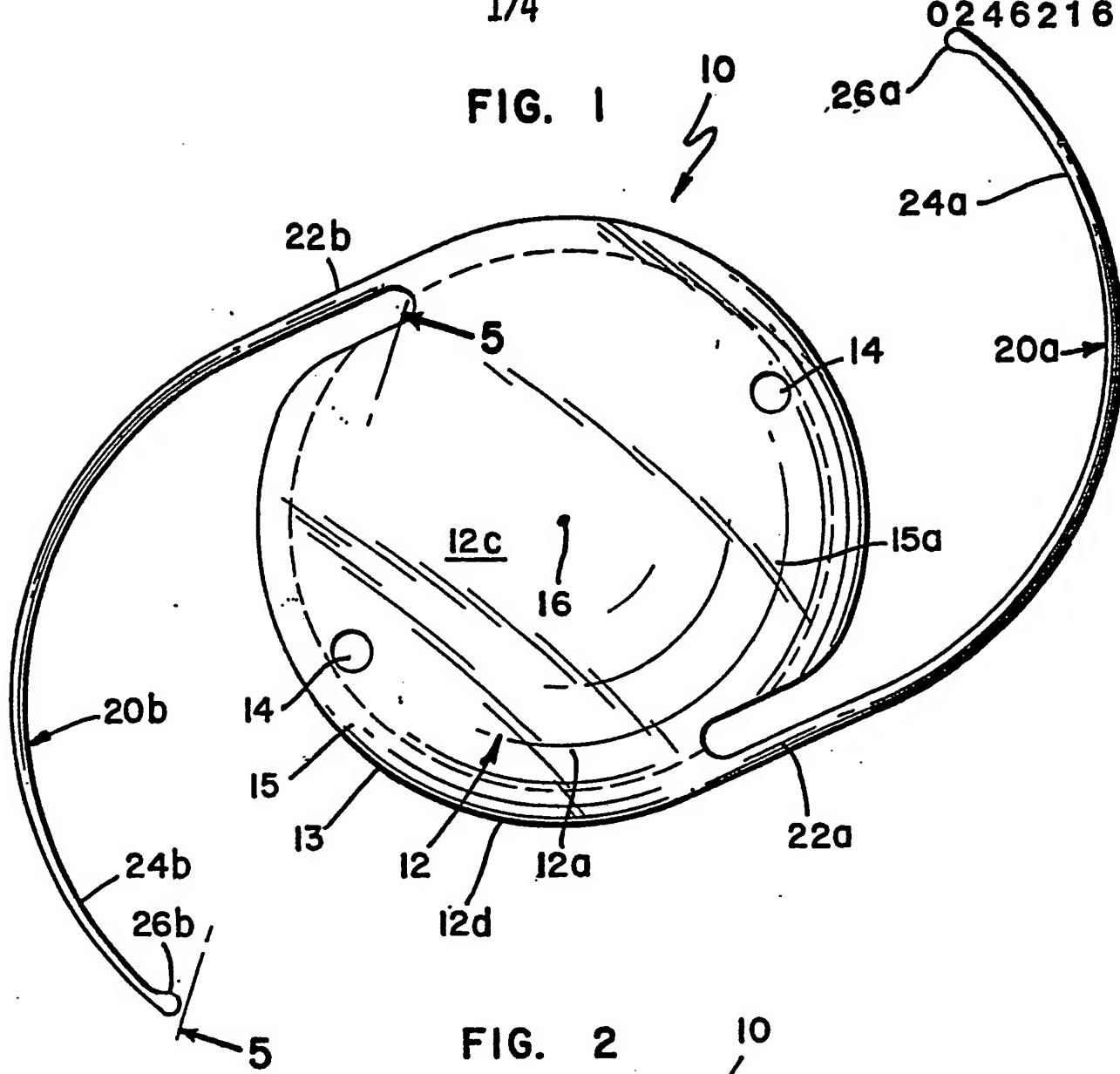


FIG. 2

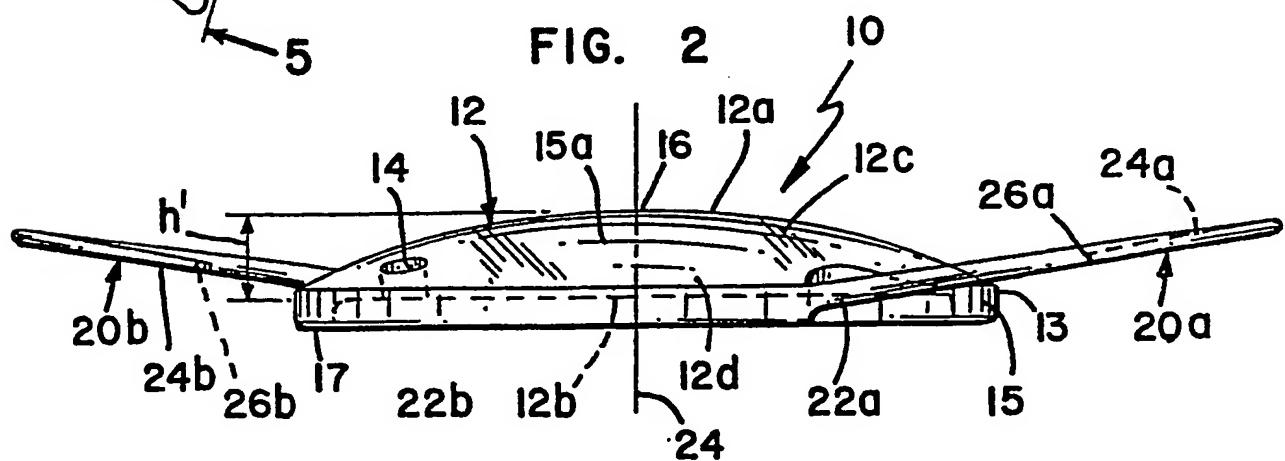
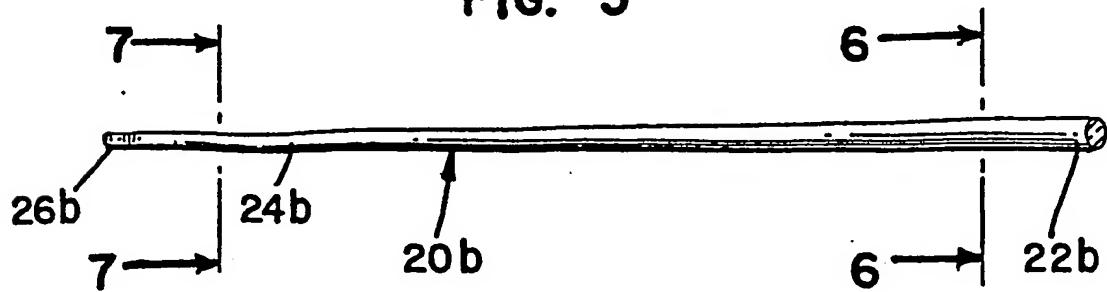


FIG. 5



2/4

0246216

FIG. 4

PRIOR ART

FIG. 3
PRIOR ART

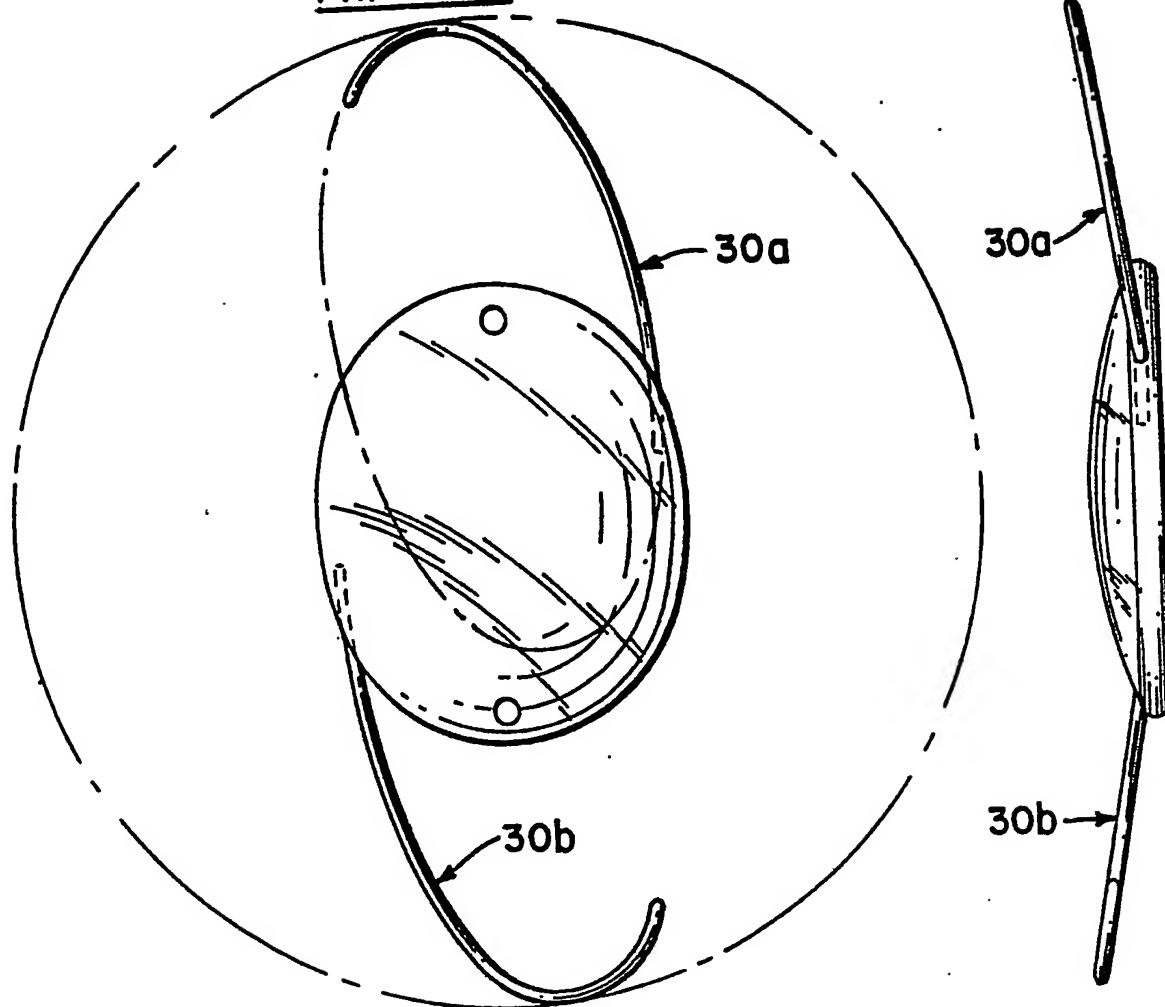
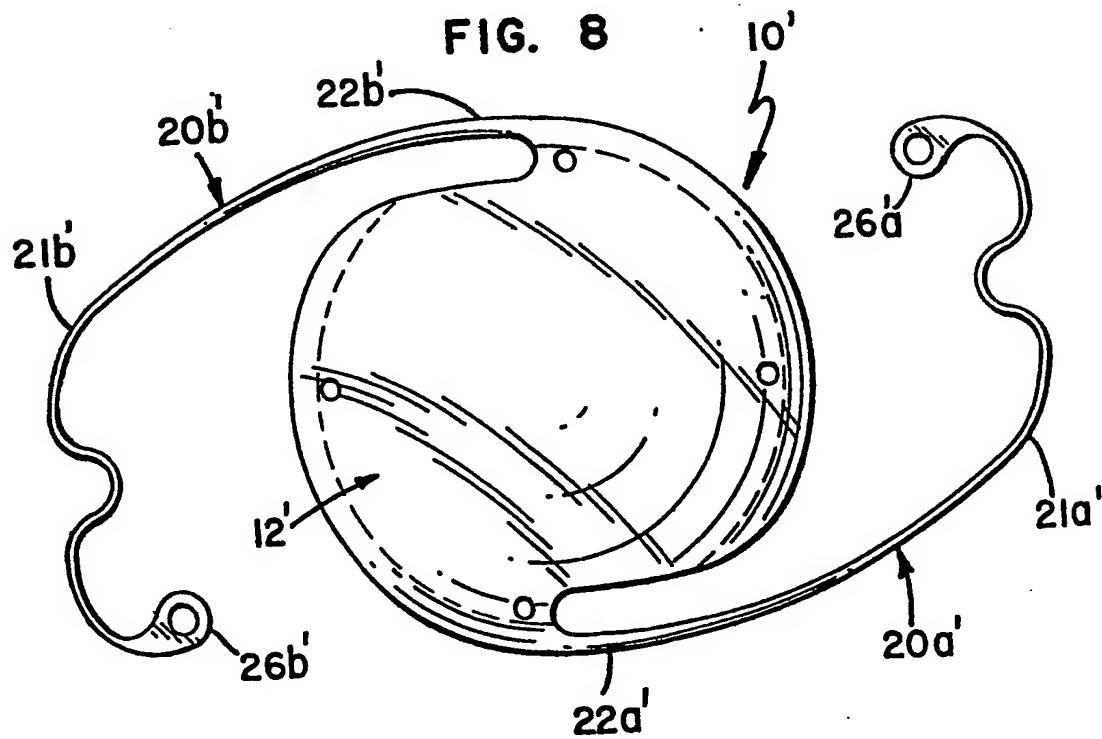


FIG. 8



3/4

0246216

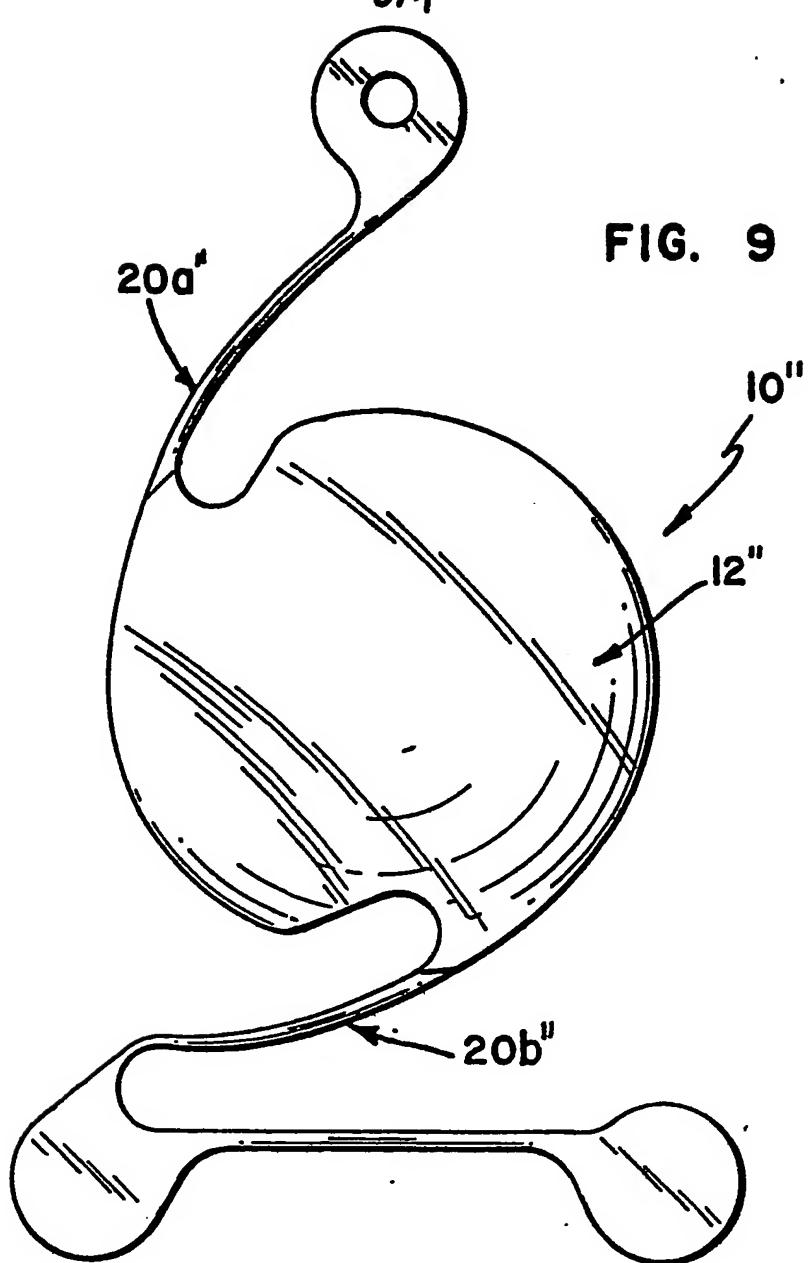


FIG. 7

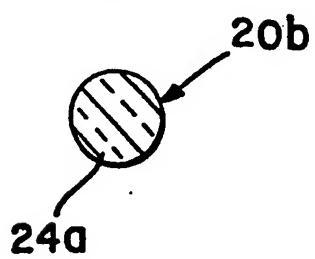


FIG. 6

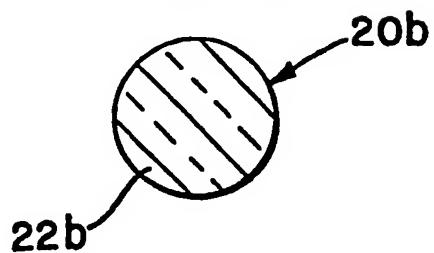


FIG. 10

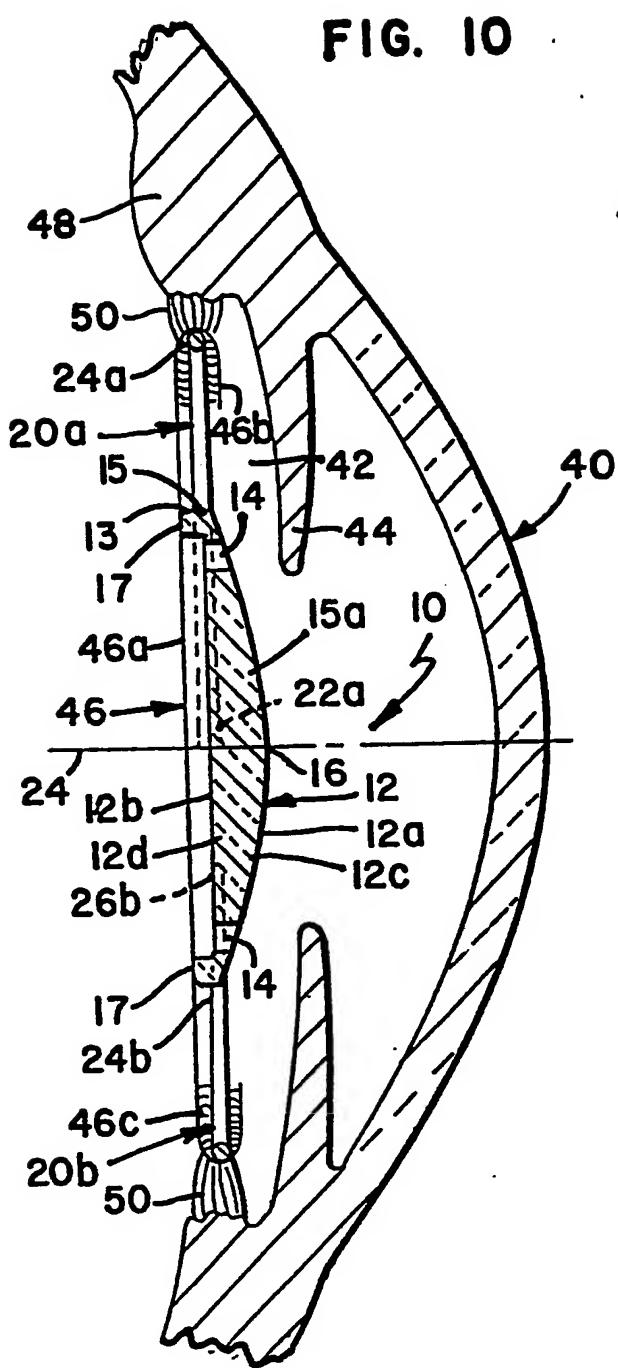


FIG. 11

